

Please amend the Claims as follows:

- an impeller; and

2. (Amended) The blood pump of Claim 1 wherein the first deformed surface lies on at least part of a first face of the impeller.

3. (Amended) The blood pump of Claim 1 wherein the second deformed surface lies on a second face of the impeller.

4. (Amended) The blood pump of Claim 1 wherein the first deformed surface lies on a first inner face of the housing.

5. (Amended) The blood pump of Claim 1 wherein the second deformed surface lies on a second inner face of the housing.

6. (Amended) The blood pump of Claim 2 wherein the first deformed surface covers entirely the first face.

7. (Amended) The blood pump of Claim 2 wherein the first deformed surface covers entirely the second face.

8. (Amended) The blood pump of Claim 1 wherein the first face lies at an acute angle relative to the second face.

9. (Amended) The blood pump of Claim 1 wherein the hydrodynamic forces are augmented by at least one secondary force to support the impeller for rotation within the housing.

10. (Amended) The blood pump of Claim 9 wherein the at least one secondary force comprises magnetic force.

11. (Amended) The blood pump of Claim 1 wherein the first deformed surface comprises deformations in the first face of the impeller whereby a gap between the first deformed surface and a first facing surface on the housing forms, in use, a restriction in the form of a reducing distance between the surfaces with respect to the relative line of movement of the first deformed surface.

12. (Amended) The blood pump of Claim 11 wherein the gap takes the form of a wedge shaped restriction which generates a thrust in use.

13. (Amended) The blood pump of Claim 1 wherein the pump is of centrifugal type or mixed flow type with impeller blades open on both front and back faces of the pump housing.

14. (Amended) The blood pump of Claim 1 wherein the front face of the pump housing is made conical, in order that the thrust perpendicular to a conical surface of the impeller has a radial component, which provides a radial restoring force to a radial displacement of the impeller axis during use.

15. (Amended) The blood pump of Claim 1 wherein the driving torque of the impeller derives from magnetic interaction between permanent magnets within blades of the impeller and oscillating currents in windings encapsulated in the pump housing.

16. (Amended) The pump of Claim 15 wherein the blades include magnetic material therein, the magnetic material being encapsulated within a biocompatible shell or coating.

17. (Amended) The pump of Claim 16 wherein the biocompatible shell or coating comprises a coating which can be applied at low temperature.

18. (Amended) The pump of Claim 16 wherein internal walls of the pump which can come into contact with the blades during use are coated with a hard material.

27. (Amended) The pump of Claim 25 further comprising a regulator in communication with the controller and the electrical drive so as to sense and inhibit under pumping and regurgitation.

34. (Amended) The system of Claim 28 wherein the pump is a low specific speed pump.

35. (Amended) The system of Claim 34 wherein the pump has a specific speed in the range 100-2000 rev/min(gal/min)^{1/2}ft^{-3/4}.

36. (Amended) The system of Claim 34 wherein the pump has a specific speed of approximately 900-1000 rev/min(gal/min)^{1/2}ft^{-3/4}.

37. (Amended) The system of Claim 28, further comprising a rotary blood pump wherein the pump has an impeller suspended hydrodynamically within a pump housing by thrust forces generated by the impeller during movement in use of the impeller as it rotates about an impeller axis;

38. (Amended) The blood pump and estimation and control system of Claim 37 wherein the thrust forces are generated by blades of the impeller.

39. (Amended) The blood pump and estimation and control system of Claim 38 wherein the thrust forces are generated by forces of the blades of the impeller.

40. (Amended) The blood pump and estimation and control system of Claim 39 wherein the blades are tapered or non-planar, so that a thrust is created between the edges and the pump housing during relative movement therebetween.

41. (Amended) The blood pump and estimation and control system of Claim 38 wherein the blades are shaped such that the gap at the leading edge of the blade is greater than at the trailing edge and thus the fluid which is drawn through the gap experiences a wedge shaped restriction which generates a thrust.

42. (Amended) The blood pump and estimation and control system of Claim 37 wherein the pump is of centrifugal type or mixed flow type with blades of the impeller open on both front and back faces of the pump housing.

44. (Amended) The blood pump and estimation and control system of Claim 38 wherein the driving torque of the impeller derives from the magnetic interaction between permanent magnets within the blades of the impeller and oscillating currents in windings encapsulated in the pump housing.

45. (Amended) The rotary blood pump and estimation and control system of Claim 37 wherein the pump is of axial type.

46. (Amended) The rotary blood pump and estimation and control system of Claim 45 wherein, within a uniform cylindrical section of the pump housing, the impeller includes tapered blade bearing surfaces which form a radial hydrodynamic bearing.

47 48. (Amended) The rotary blood pump and estimation and control system of Claim 46 wherein magnetic forces provide the axial bearing.

48 49. (Amended) The rotary blood pump and estimation and control system of Claim 37, further comprising a housing within which an impeller acts by rotation about an impeller axis to cause a pressure differential between an inlet side of the pump housing of the pump and an outlet side of the pump housing of the pump, wherein the impeller is suspended hydrodynamically by thrust forces generated by the impeller during movement in use of the impeller

49 50. (Amended) The rotary blood pump and estimation and control system of Claim 48 49 wherein the impeller includes magnetic material therein, the magnetic material encapsulated within a biocompatible shell or coating.

50 51. (Amended) The rotary blood pump and estimation and control system of Claim 49 50 wherein the biocompatible shell or coating comprises of a material which can be applied at low temperature.

51 52. (Amended) The rotary blood pump and estimation and control system of Claim 48 49 wherein internal walls of the pump which can come into contact with the blades during use are coated with a hard material.

52 53. (Amended) The rotary blood pump and estimation and control system of Claim 37, wherein the pump is seal-less and shaft-less pump and comprises a housing defining a chamber therein and having a liquid inlet to the chamber and a liquid outlet from the chamber; the pump further including an impeller located within the chamber; the arrangement between the impeller, the inlet, the outlet and the internal walls of the chamber being such that upon rotation of the impeller about an impeller axis relative to the housing, liquid is urged from the inlet through the chamber to the outlet; and wherein thrust forces are generated by relative movement of the impeller with respect to the housing

53 54. (Amended) The pump of Claim ⁵²53 wherein the thrust forces are generated by blades of the impeller.

54 55. (Amended) The pump of Claim ⁵³54 wherein the thrust forces are generated by surfaces of the blades of the impeller.

55 56. (Amended) The pump of Claim ⁵⁴55 wherein the surfaces of the blades are tapered or non-planar.

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56 ~~57~~. (Amended) The pump of Claim ~~53~~ wherein the surfaces of the blades are shaped such that a gap at the leading edge of each of the blades is greater than at a trailing edge thereof whereby fluid which is drawn through the gap experiences a wedge shaped restriction which generates a thrust relative to the housing.

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57 ~~58~~. (Amended) The pump of Claim ~~54~~ wherein the pump is of centrifugal type or mixed flow type with the blades of the impeller open on both front and back faces of the pump housing.

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58 ~~60~~. (Amended) The pump of Claim ~~58~~ wherein the driving torque of the impeller derives from the magnetic interaction between permanent magnets within the blades of the impeller and oscillating currents in windings encapsulated in the pump housing.

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59 ~~61~~. (Amended) The pump of Claim ~~53~~ wherein the pump is of axial type.

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60 ~~62~~. (Amended) The pump of Claim ~~61~~ wherein, within a uniform cylindrical section of the pump housing, tapered blade surfaces form a radial hydrodynamic bearing.

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61 ~~64~~. (Amended) The pump of Claim ~~61~~ wherein magnetic forces provide the axial bearing.

62 ~~65~~. (Amended) The rotary blood pump and estimation and control system of Claim ~~48~~ 49, wherein the impeller is suspended hydrodynamically in at least one of a radial or axial direction by thrust forces generated by the impeller during movement in use of the impeller

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63 ~~66~~. (Amended) The pump of Claim ~~65~~ wherein the impeller includes magnetic material therein, the magnetic material encapsulated within a biocompatible shell or coating.

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64 ~~67~~. (Amended) The pump of Claim ~~66~~ wherein the biocompatible shell or coating comprises a diamond coating.

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65 ~~68~~. (Amended) The pump of Claim ~~66~~ wherein internal walls of the pump which can come into contact with the impeller during use are coated with a hard material.

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66 ~~69~~. (Amended) The pump of Claim ~~65~~ wherein at least upper and lower surfaces of blades of the impeller are interconnected by a structure having deformities in the outer surfaces thereof so that a thrust is created between the surfaces and the adjacent pump casing during relative movement therebetween.

67 ~~70~~. (Amended) A method of hydrodynamically suspending and controlling an impeller within a rotary pump for support in at least one of a radial and axial direction; the method comprising:

incorporating a deformed surface, in at least part of the impeller so that, in use, a thrust is created between the deformed surface and an adjacent pump housing during relative movement therebetween; and

maintaining the speed of rotation of the impeller within a range whereby the impeller, in use, substantially resists five degrees of freedom of movement with respect to the pump housing without any external intervention.

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~~68~~ 71. (Amended) The method of Claim ~~70~~ wherein the deformed surface includes a taper.

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~~69~~ 72. (Amended) The method of Claim ~~71~~ wherein the taper is arranged so that there is a larger gap at a leading edge thereof between the impeller and the pump housing than at a trailing edge thereof.

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~~70~~ 73. (Amended) An estimation and control system for a pump; the pump of the type having an impeller located within a pump cavity in a pump housing; the housing having a fluid inlet in fluid communication with the cavity; the housing having a fluid outlet in fluid communication with the pump cavity; the impeller urged to rotate about an impeller axis so as to cause fluid to be urged from the inlet through the pump cavity to the pump outlet; the impeller urged to rotate by an impeller drive; impeller supported for rotational movement by an impeller support; the pump maintained at or near a predetermined operating point by a controller acting on the impeller drive; the controller receiving as input variables at least a first input variable derived from the impeller drive; the controller receiving at least a second input variable also derived from the impeller drive; the controller thereby calculating an estimate of the operating point to an approximation of predetermined accuracy relying on signals available from the impeller drive; the controller controlling the pump by comparing the predetermined operating point with the estimate of the operating point; and wherein instantaneous pump speed and electrical input power are allowed to be modulated by a heart, in use, by appropriate selection of a control time constant.

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~~71~~ 74. (Amended) The system of Claim ~~73~~ in combination with the pump.

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~~72~~ 75. (Amended) The system of Claim ~~73~~ wherein the control time constant of the control system is greater than the rotational, inertial time constant of the impeller.

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~~73~~ 76. (Amended) The system of Claim ~~73~~ wherein the control time constant is at least one cardiac cycle.

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85 88. (Amended) The controller of Claim ⁸⁴88 wherein the processor calculates flow and head to discern optimal pumping based on collapse and overpumping.

86 90. (Amended) The controller of Claim ⁸⁴88 wherein the processor calculates values of speed and power (peak and RMS values) to discern optimal pumping based on collapse and overpumping.

87 91. (Amended) The controller of Claim ⁸⁴88 wherein the processor includes a control aim which adjusts optimal pump output to a point close to where the aortic valve just opens or just fails to open.

88 92. (Amended) The controller of Claim ⁸⁷91 wherein the pump comprises a ventricular assist device adapted to assist operation of a ventricle of a heart and wherein the processor adjusts pump output so that, in alternating fashion, the ventricle in conjunction with the aortic valve is allowed to eject blood over a predetermined number of cardiac cycles and then the ventricle in conjunction with the aortic valve is caused to not eject blood over a following predetermined number of cardiac cycles.

89 93. (Amended) An estimation and control system for a pump; the pump of the type having an impeller located within a pump cavity in a pump housing; the housing having a fluid inlet in fluid communication with the cavity; the housing having a fluid outlet in fluid communication with the pump cavity; the impeller urged to rotate about an impeller axis so as to cause fluid to be urged from the inlet through the pump cavity to the pump outlet; the impeller urged to rotate by an impeller drive; the impeller supported for rotational movement by an impeller support; the pump maintained at or near a predetermined operating point by a controller acting on the impeller drive; the controller receiving as input variables at least a first input variable derived from the impeller drive; the controller receiving at least a second input variable also derived from the impeller drive; the controller thereby calculating an estimate of the operating point to an approximation of predetermined accuracy relying on signals available from the impeller drive; the controller controlling the pump by comparing the predetermined operating point with the estimate of the operating point; and wherein the pump is arranged to operate according to a relatively flat HQ characteristic.

90 94. (Amended) The estimation and control system of Claim ⁸⁹93 wherein there is no inflexion point in the HQ characteristic at or near the predetermined operating point.

91 93. (Amended) The estimation and control system of Claim 93 wherein the pump includes near-radial off-flow from the impeller.

92 96. (Amended) The estimation and control system of Claim 93 wherein the pump has a low specific speed.

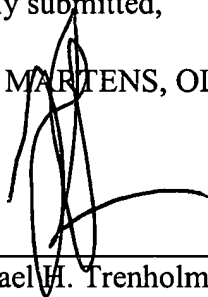
Attached hereto is a marked-up version of the changes made to the claims by the current amendment. The attached page is captioned "Version with Markings to Show Changes Made"; additions are shown as underlined and deletions are shown [bracketed].

Please charge any additional fees, including any fees for additional extension of time, or credit overpayment to Deposit Account No. 11-1410.

Respectfully submitted,

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